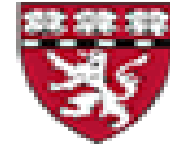


# Flow Cytometry SRL



**Beth Israel Deaconess  
Medical Center**



**Harvard  
Medical School  
Teaching Affiliate**

Vasilis Toxavidis, John Tigges, Virginia Camacho, and Gaenna Rogers

<http://www.bidmc.org/Research/CoreFacilities/FlowCytometryCore.aspx>

<http://bidflow.calendarhost.com/cgi-bin/calweb/calweb.cgi>

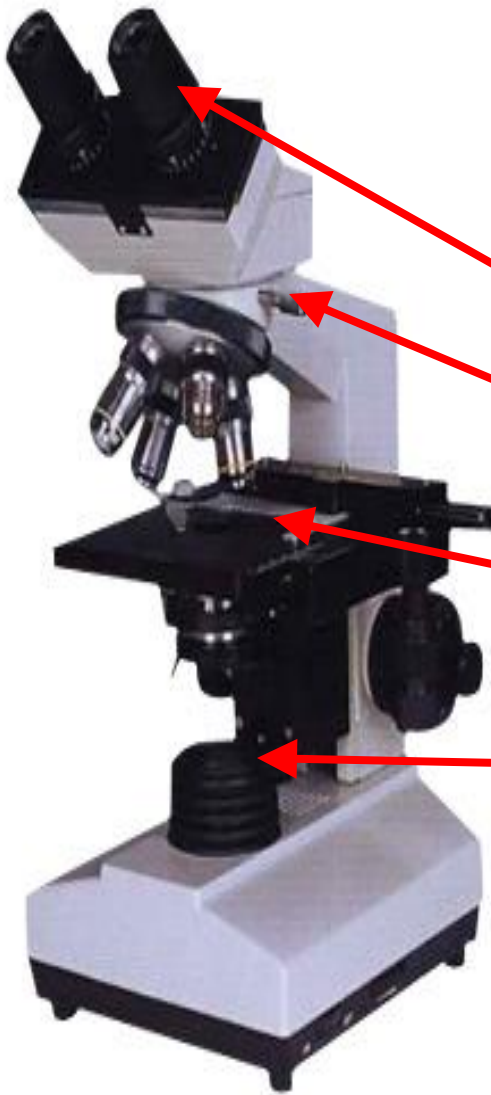
# Flow Cytometry

**Flow ~ fluid in motion**

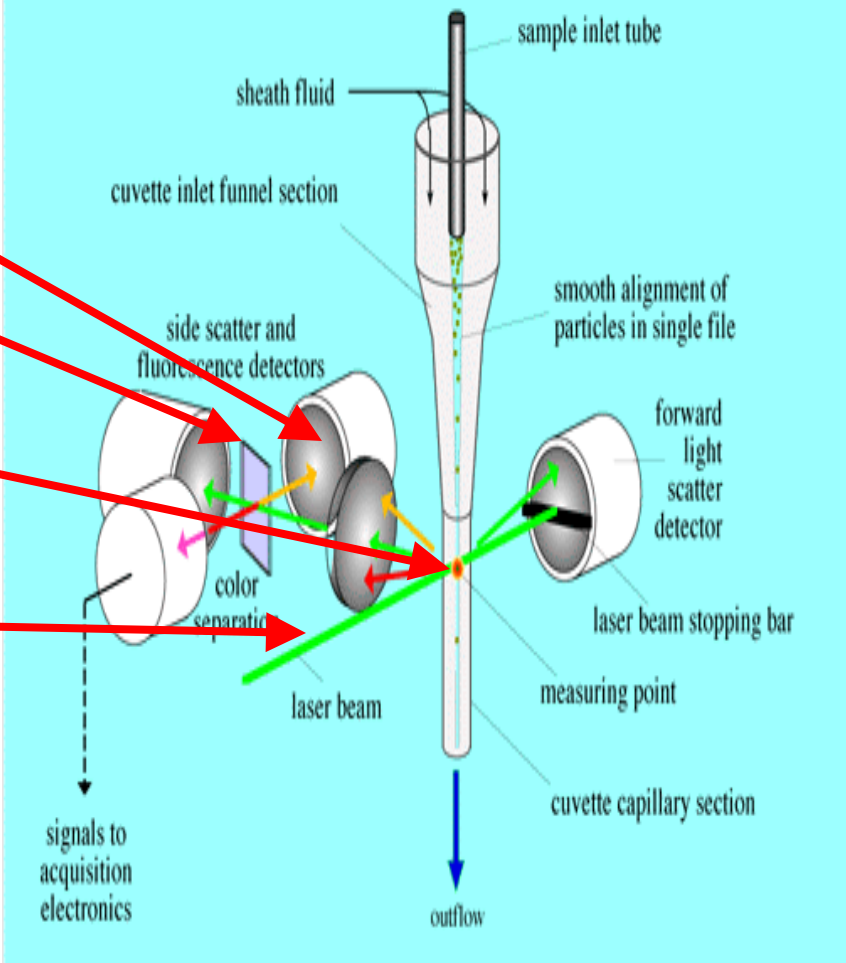
**Cyto ~ cell**

**Metry ~ measure**

**Measuring properties of cells while  
in a fluid stream**

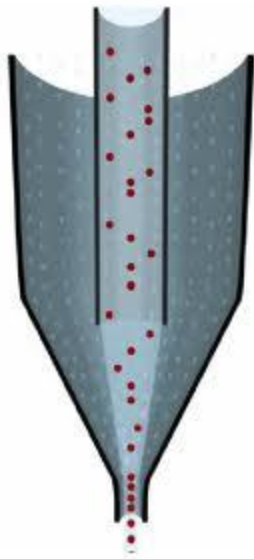


## Flow cytometer operating principle

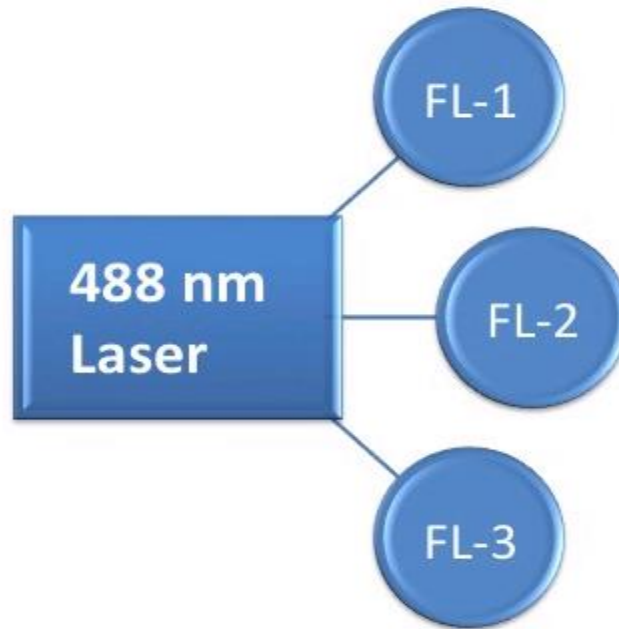


# Three main systems that make up a Flow Cytometer

## FLUIDICS



## OPTICS



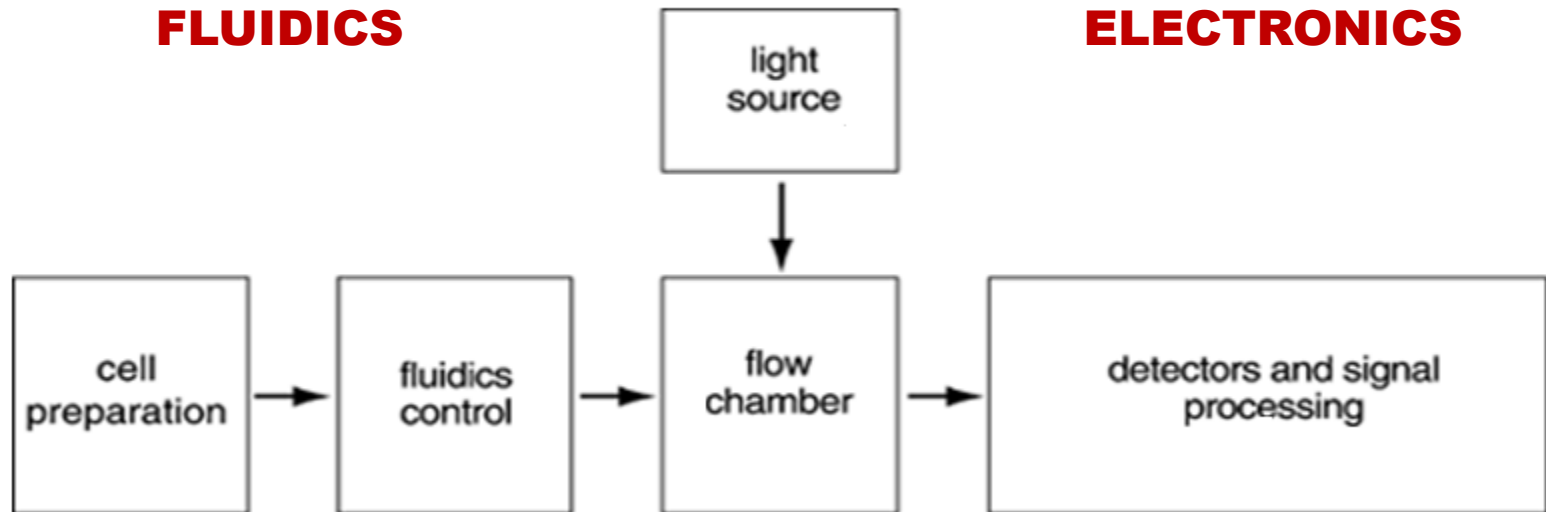
## ELECTRONICS

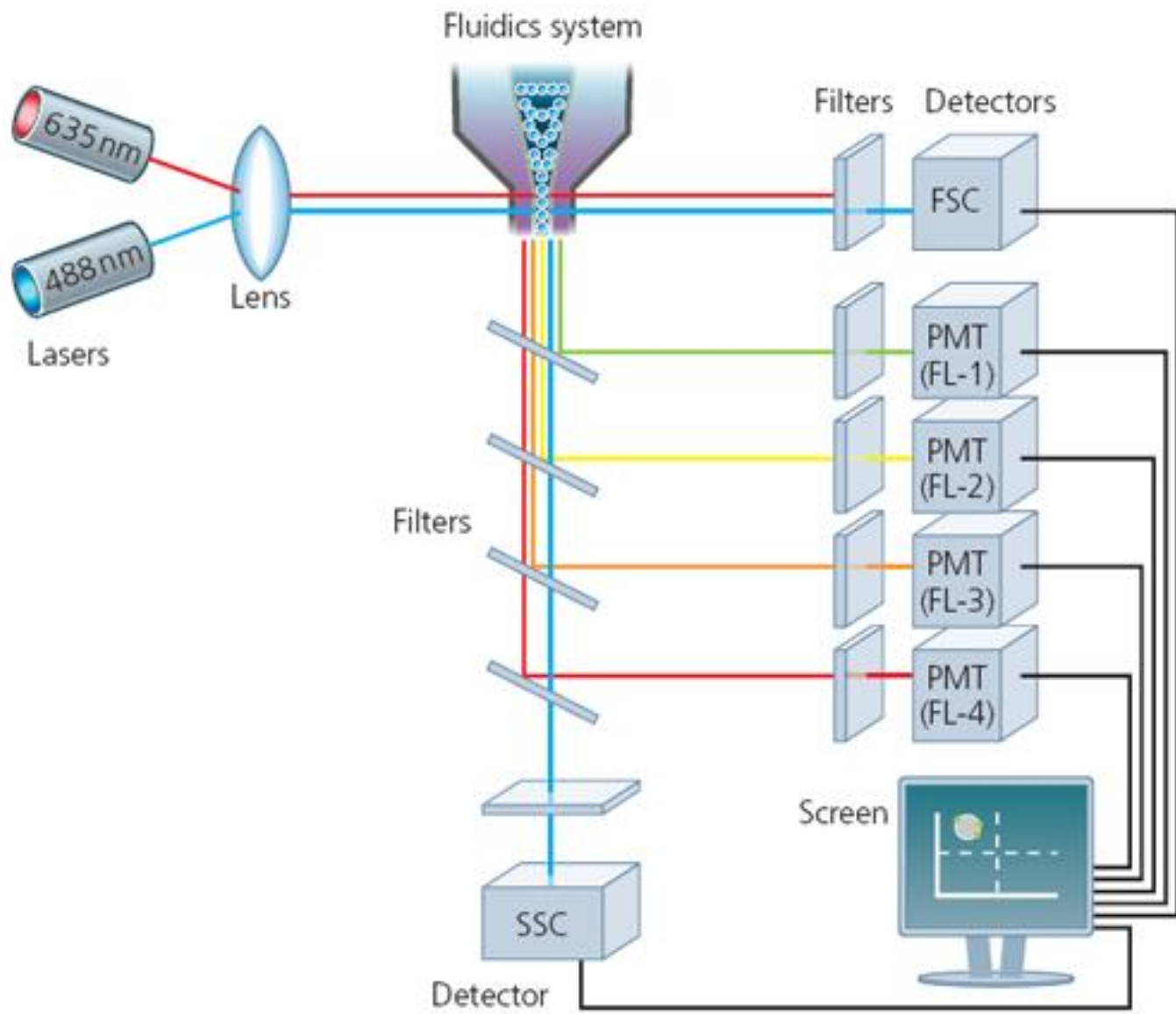


## **OPTICS**

## **FLUIDICS**

## **ELECTRONICS**

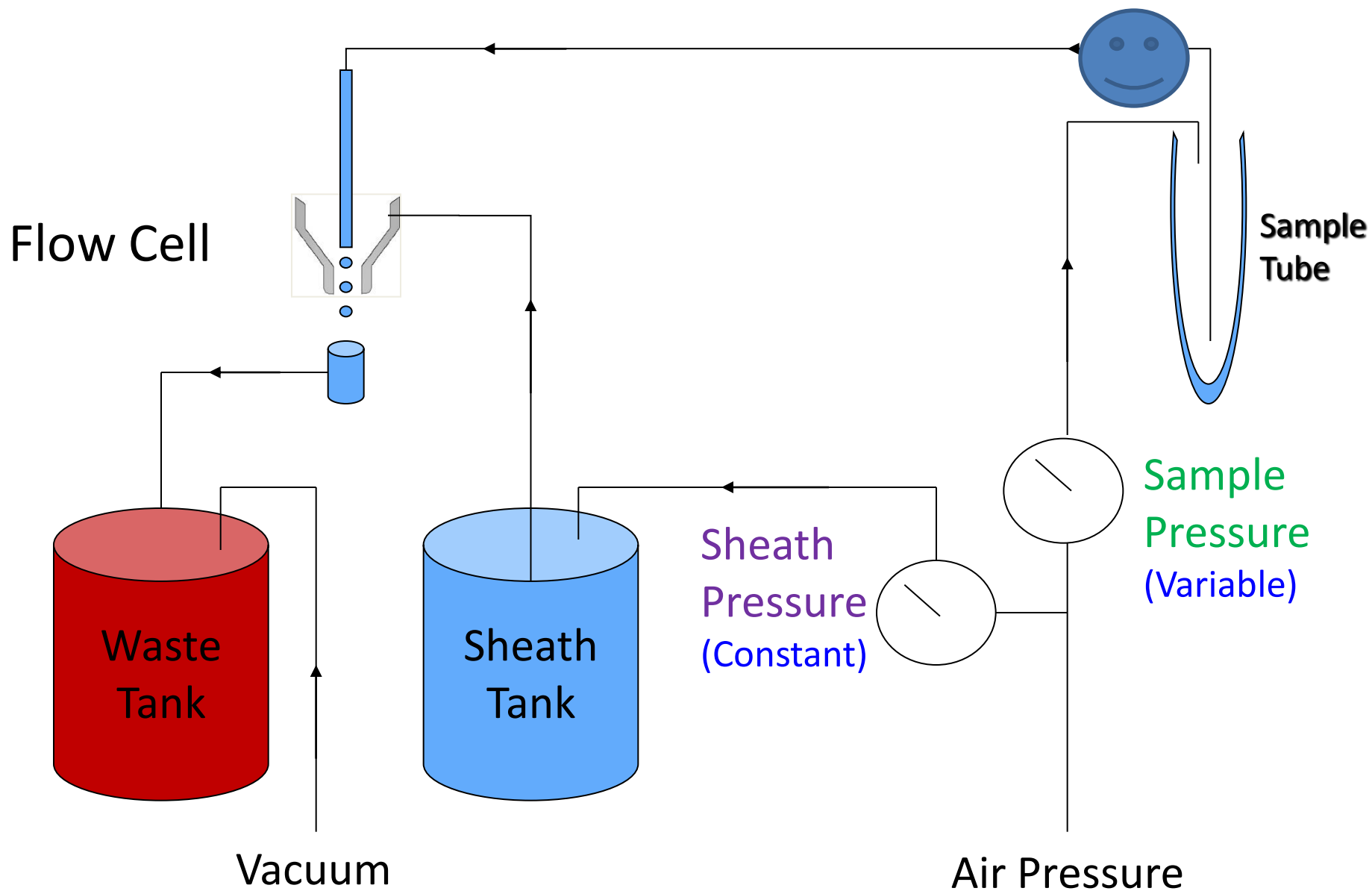




# FLUIDICS



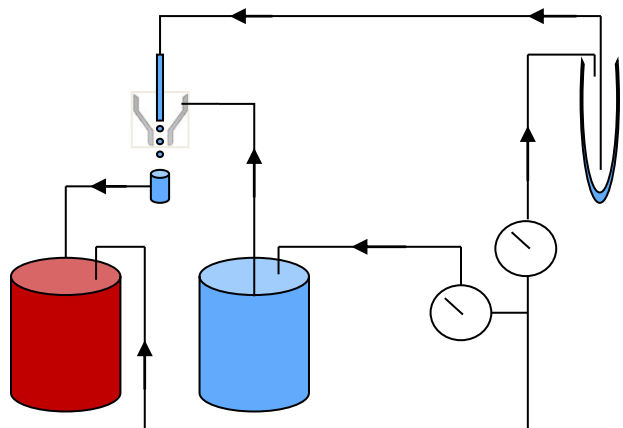
# Fluidics Schematic



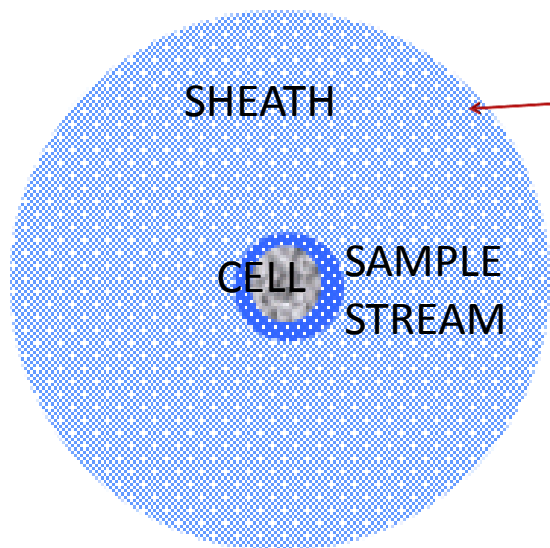
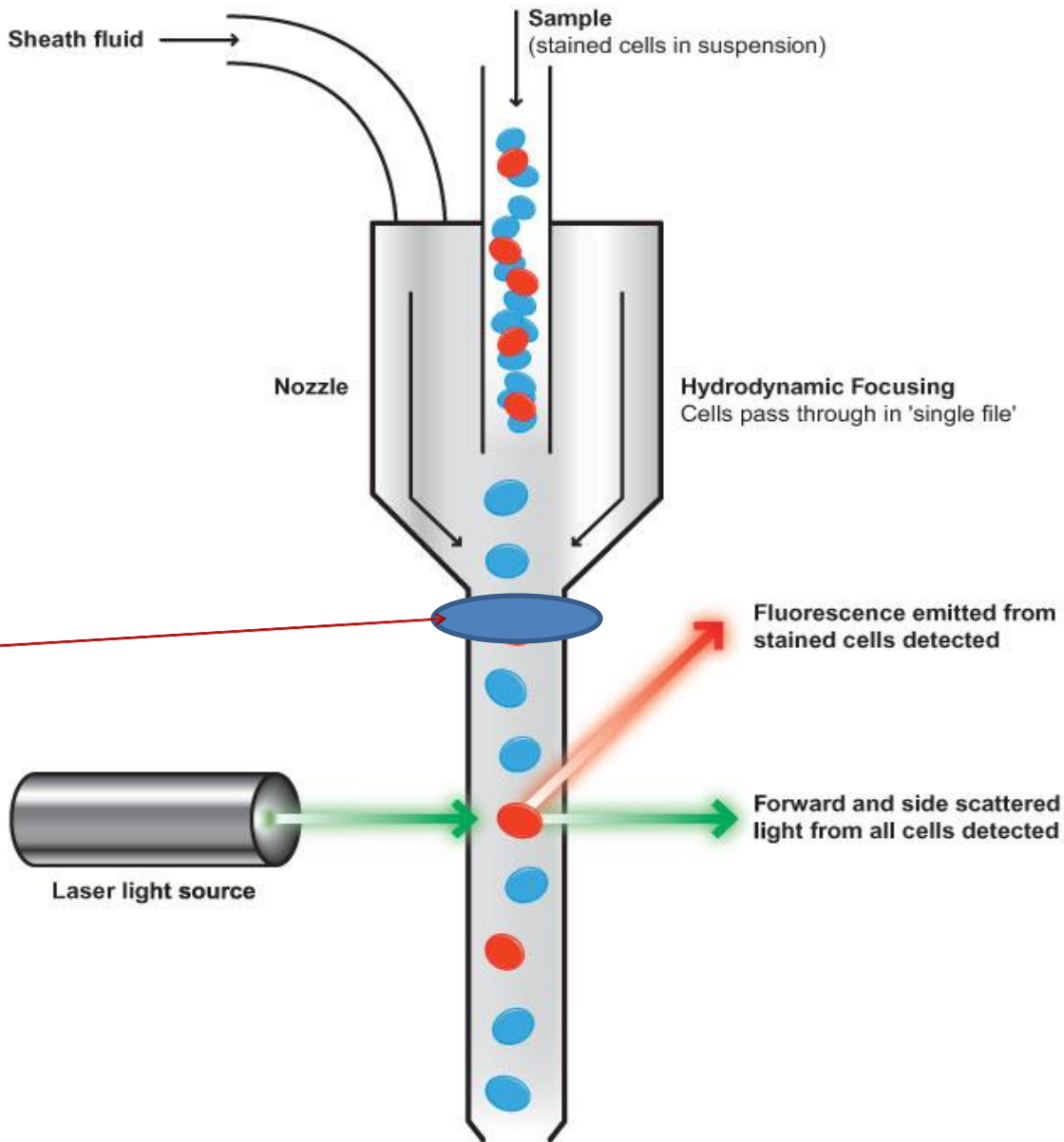


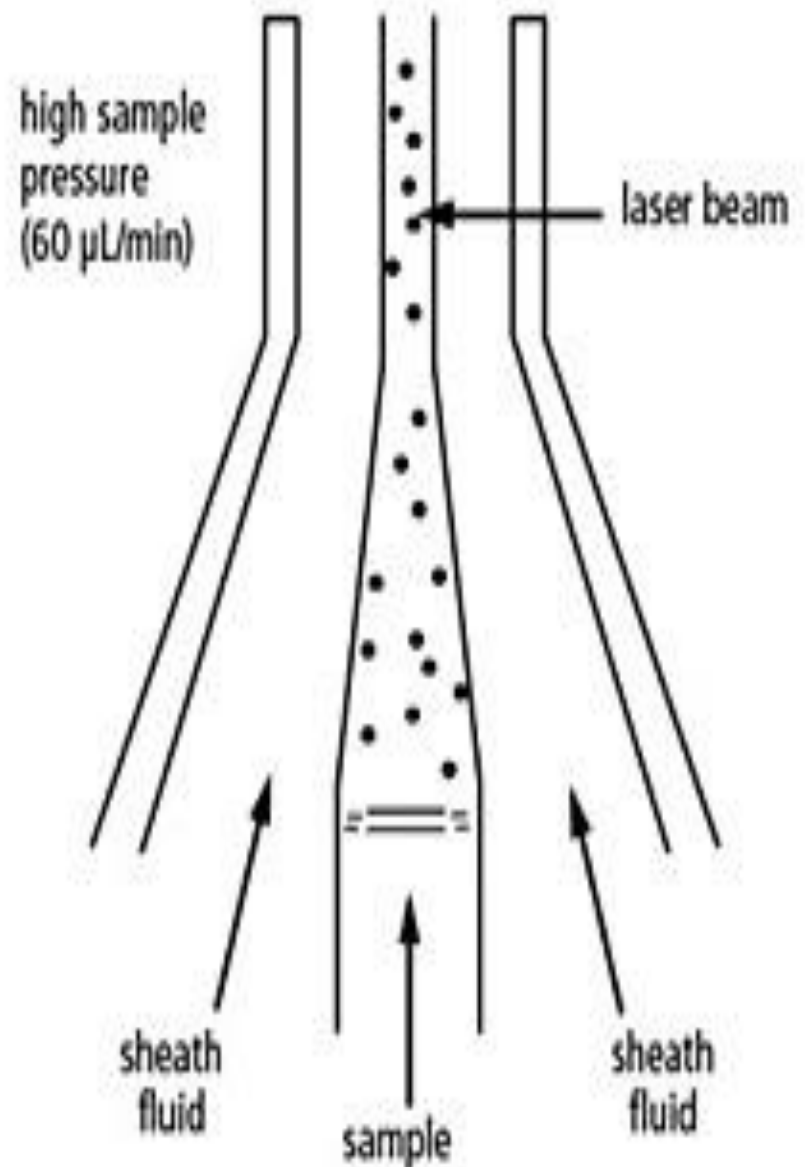
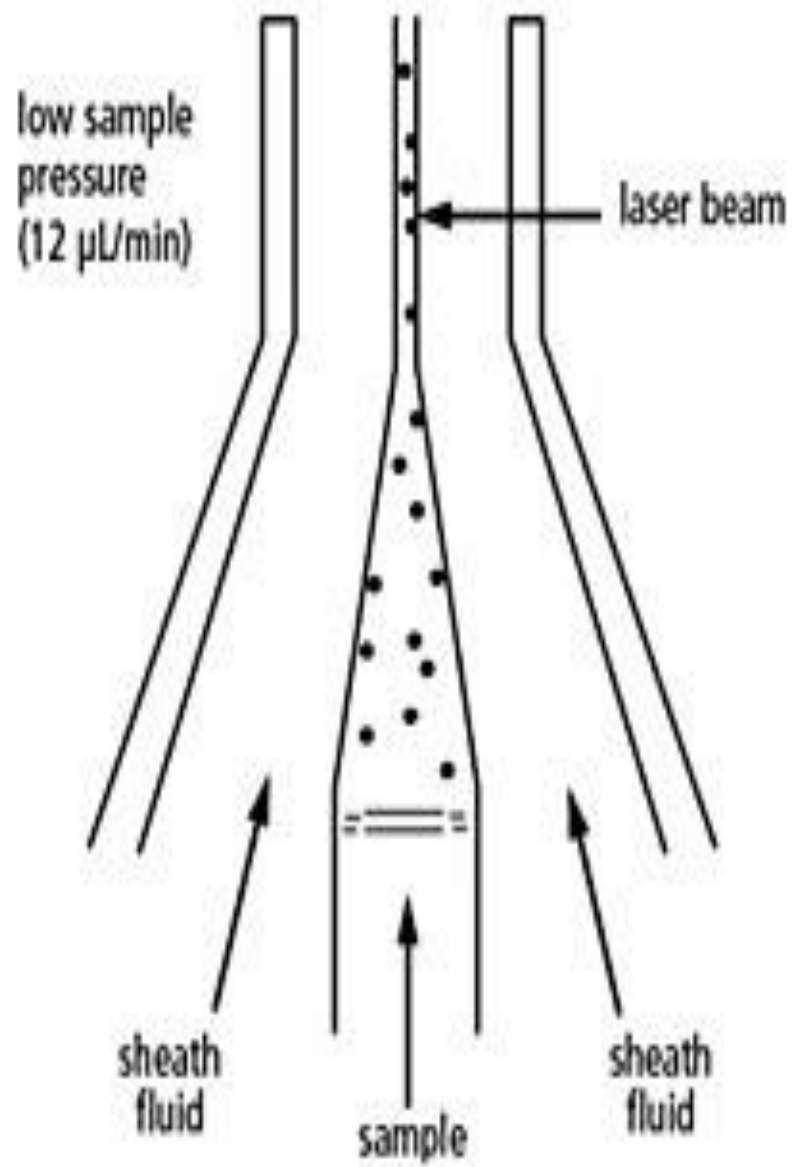
# How The Flow Cell Works

- The cells from the sample tube are injected into the sheath stream
- Flow in a flow cell is laminar.
- Hydrodynamic focusing pushes the cells to line up single file along their long axis.
- The shape of the flow cell provides the means for hydrodynamic focusing.



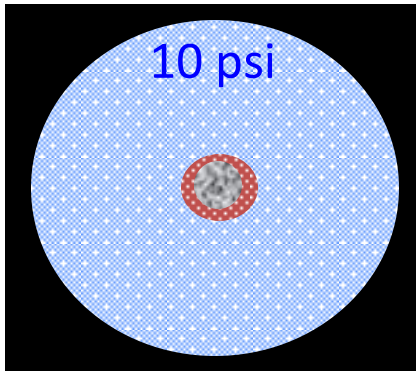
## Flow Cytometry



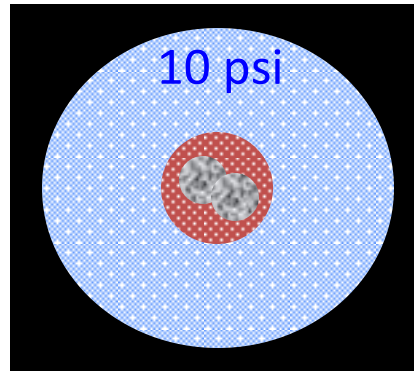


# Sample Differential

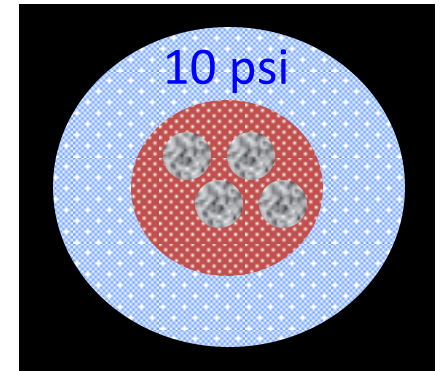
10.2 psi



10.4 psi



10.8 psi



Difference in pressure between sample and sheath

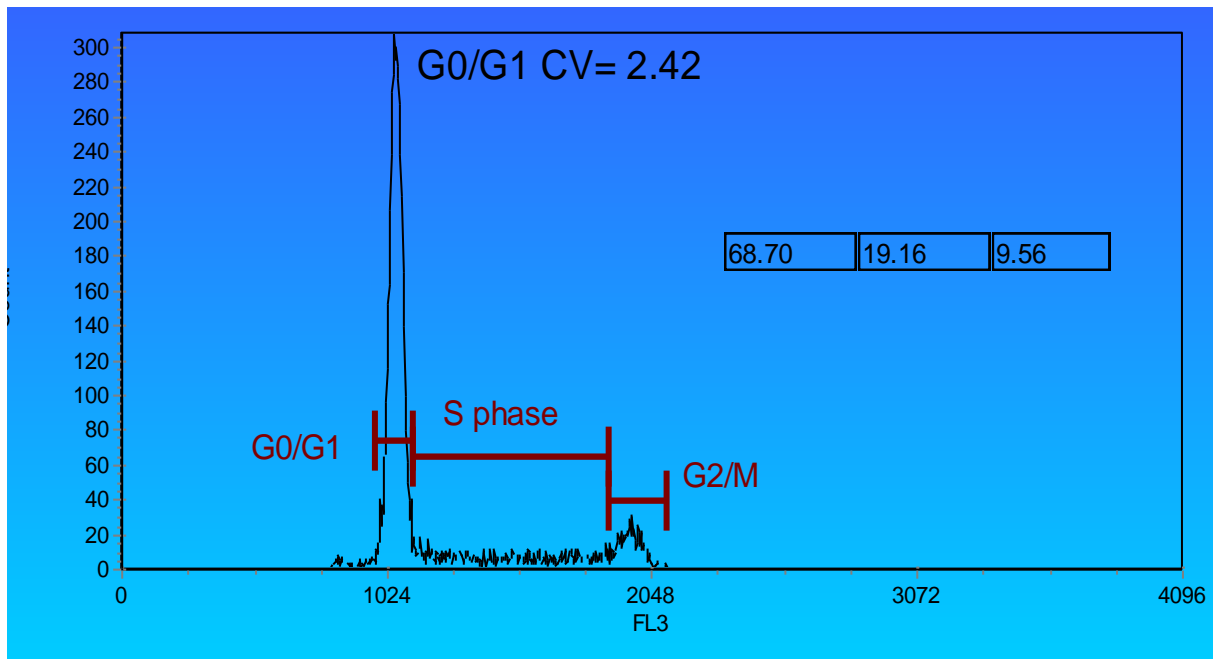
This will control sample volume flow rate

The greater the differential, the wider the sample core.

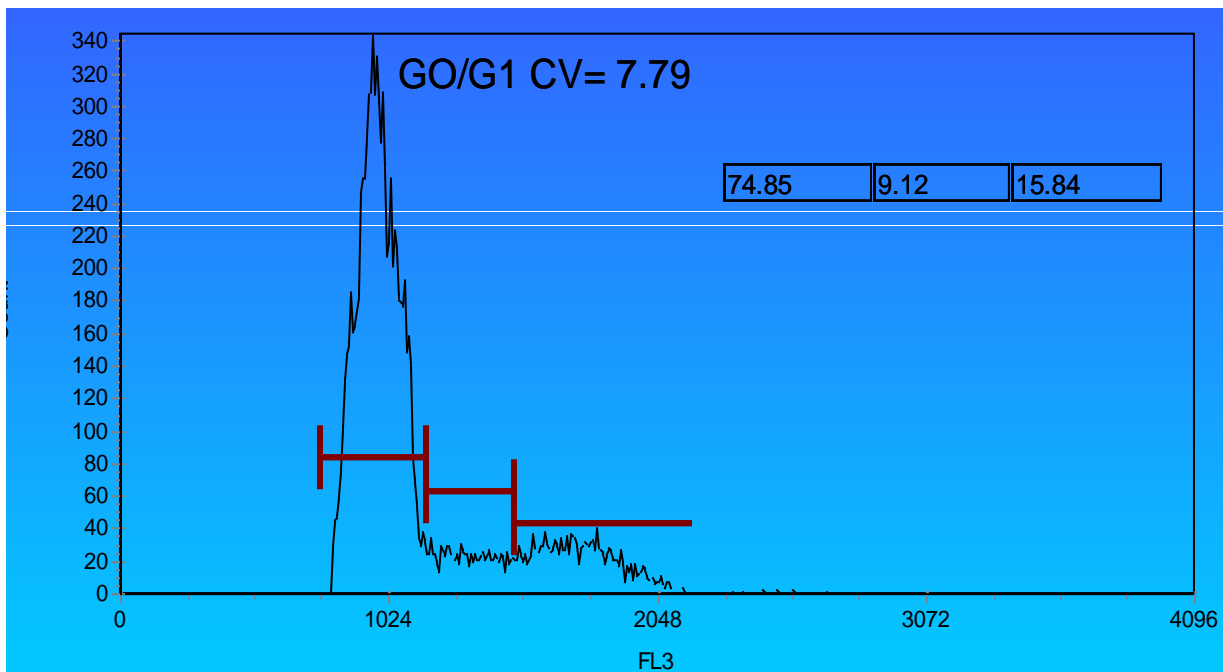
If differential is too large, cells will no longer line up single file

Results in wider **CV's** and increase in multiple cells passing through the laser at once. No more single cell analysis!

Low pressure



High pressure



# Fluidics Recap

- Purpose is to have cells flow one-by-one past a light source.
- Cells move out of tube because there is slightly greater pressure on the sample than on the sheath
- Cells are “focused” due to hydrodynamic focusing and laminar flow.

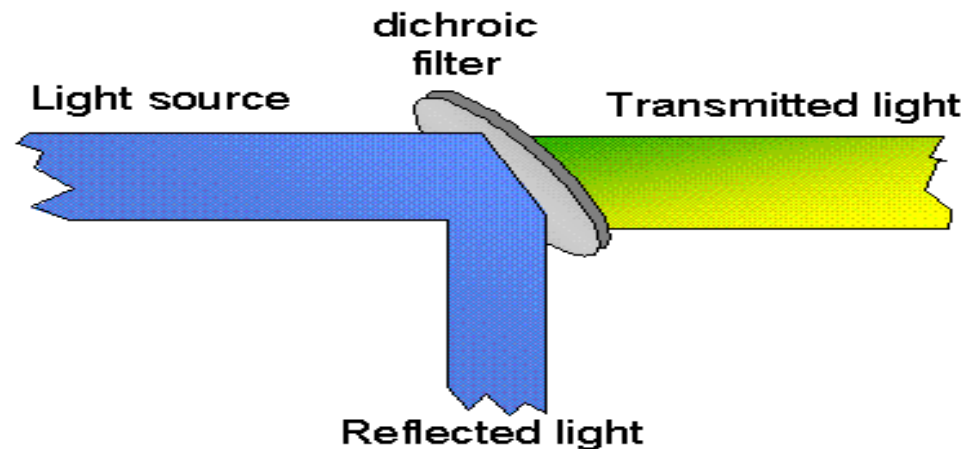
# OPTICS



# Filters

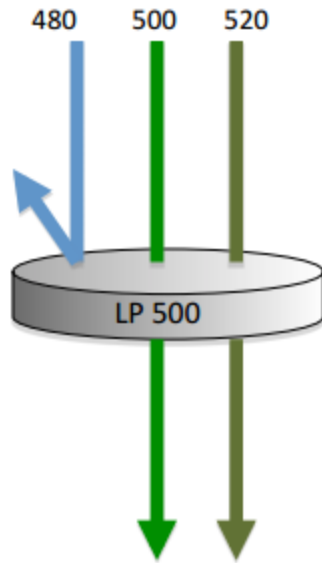


- Many wavelengths of light will be scattered from a cell, we need a way to split the light into its specific wavelengths in order to detect them independently. This is done with filters
- Optical filters are designed such that they absorb or reflect some wavelengths of light, while transmitting other.
- 3 types of filters
  - Long Pass filter
  - Short Pass filter
  - Band Pass filter



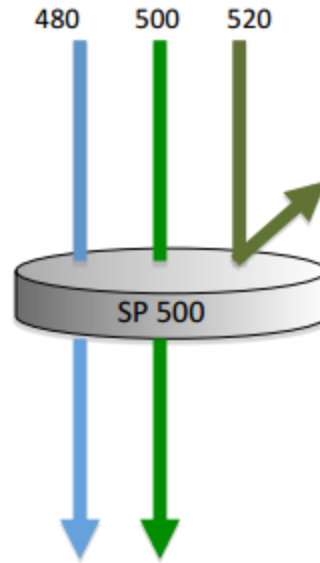


### Longpass



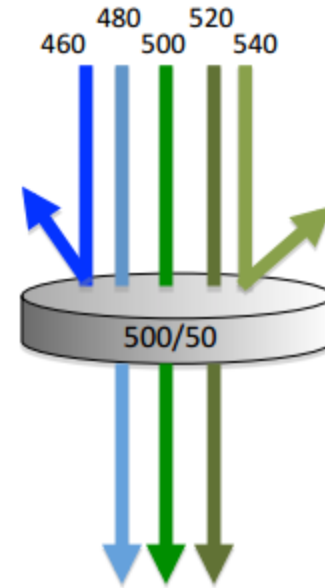
Transmits all wavelengths greater than specified wavelength

### Shortpass



Transmits all wavelengths less than specified wavelength

### Bandpass



Transmits a specific band of wavelengths  
i.e.  $500/50 = 475-525 \text{ nm}$   
( $500 \pm 25$ )

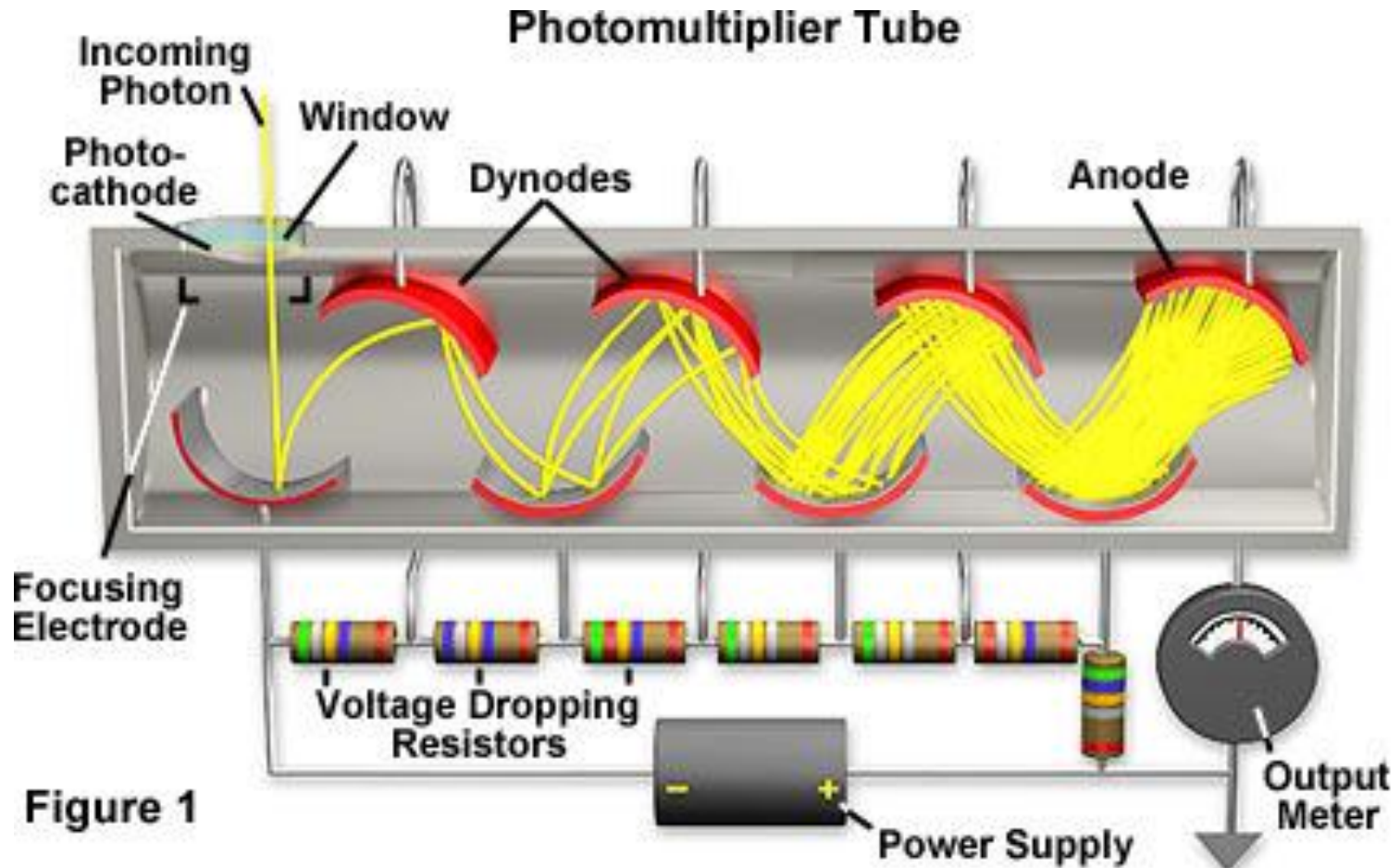
# PhotoMultiplier Tube



## Photomultiplier tubes (PMTs)

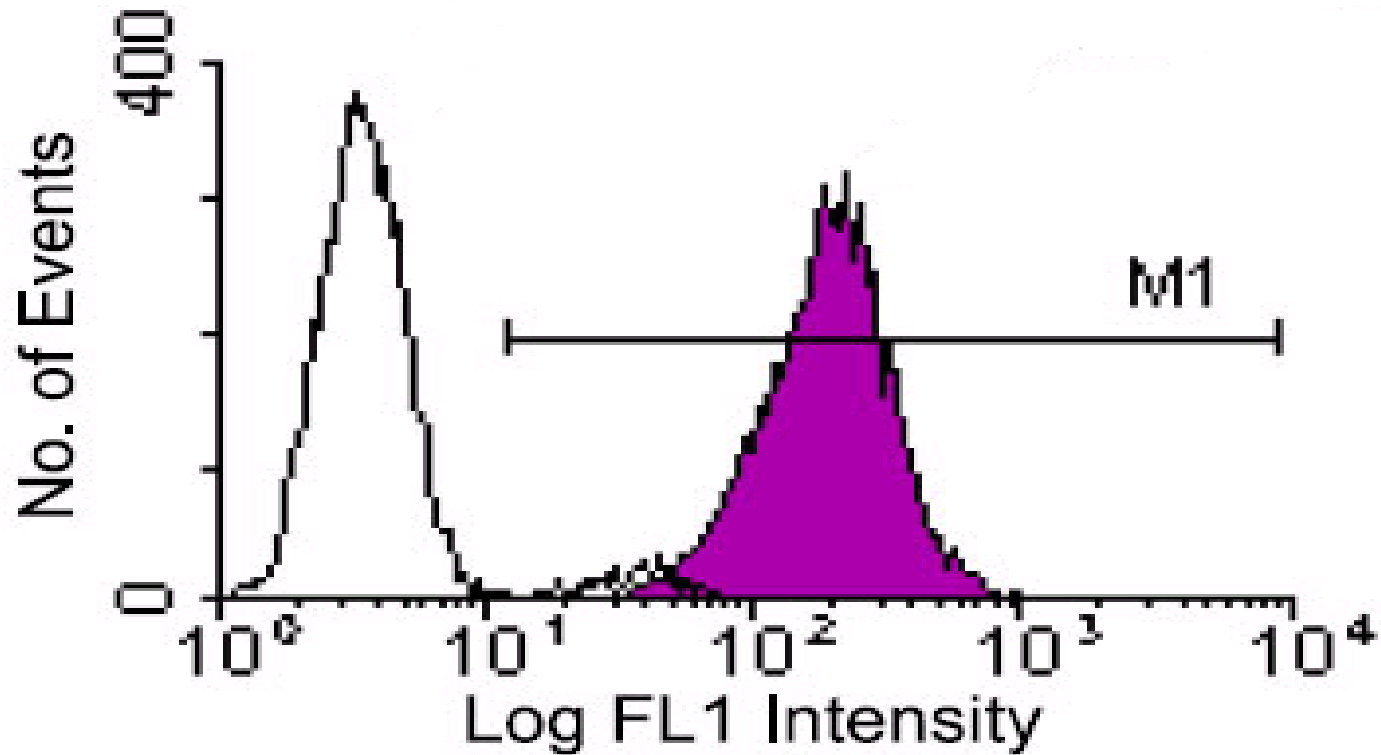
- [vacuum tubes](#), [phototubes](#)
- detect [ultraviolet](#), [visible](#), and [near-infrared](#) ranges
- Multiply the current produced by as much as 100 million times enabling [photons](#) to be detected when light is very low.

# PhotoMultiplier Tube



E.

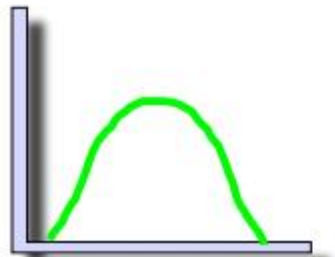
# PMT Adjustment for AutoFluorescence



Current produced by the PMT generates a voltage pulse; these electrical signals are digitized using Analog to Digital Converters (ADCs).

# Data Collection & Display

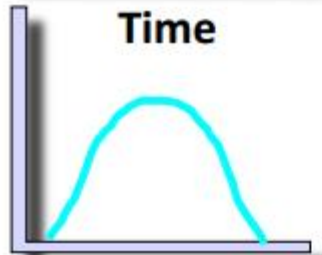
and generates histograms, dot plots, and FCS 3.0 files (Flow Cytometry Standard).



Time

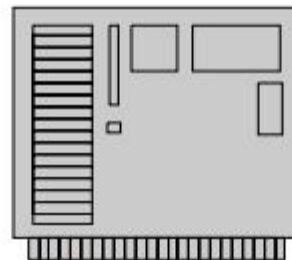


Time

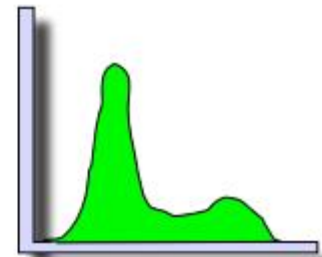


Time

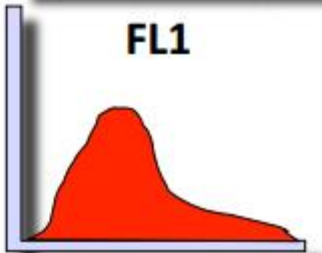
Digitized signals are processed by additional electronics that calculate peak, area, and width signals..



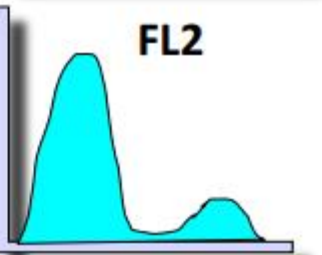
Data  
Processor



FL1



FL2



FL3

# Amplifiers

- The current exiting the detector passes through either a linear or log amplifier converting it into a voltage pulse.
- You can adjust the intensity of the voltage by amplifying it on a linear or log scale

# Linear Amplifiers

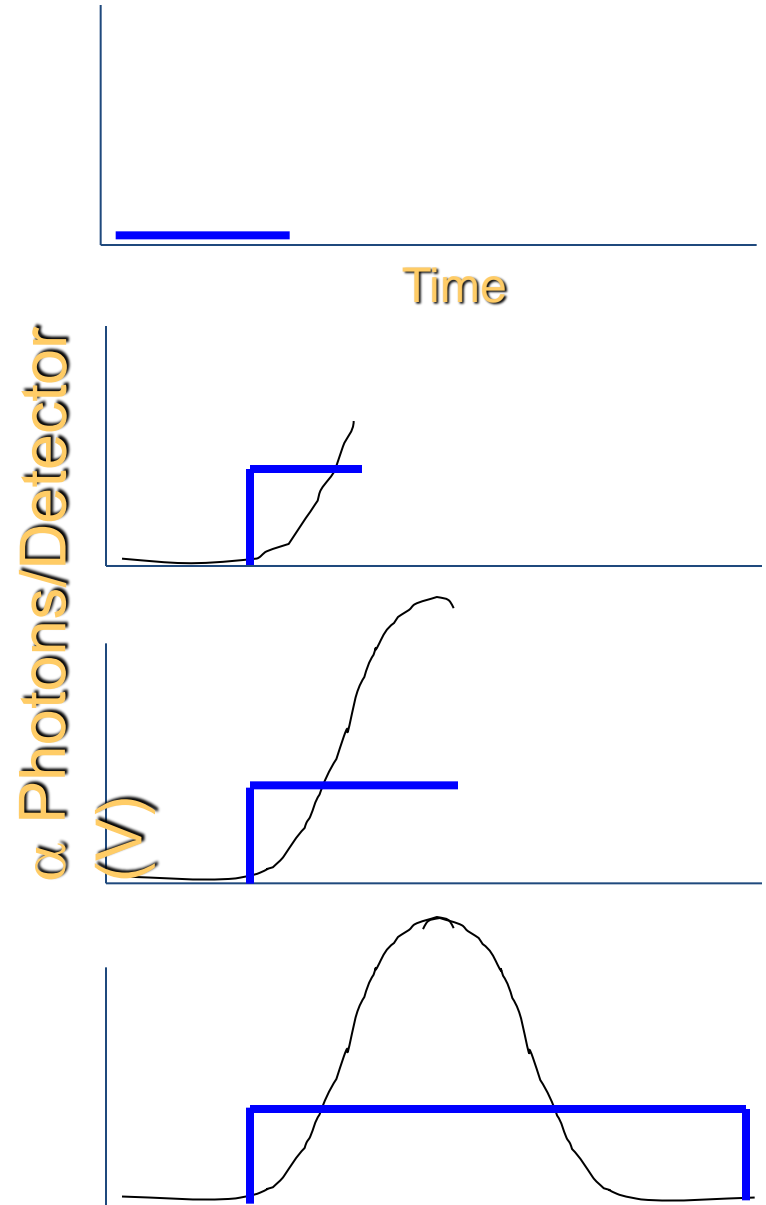
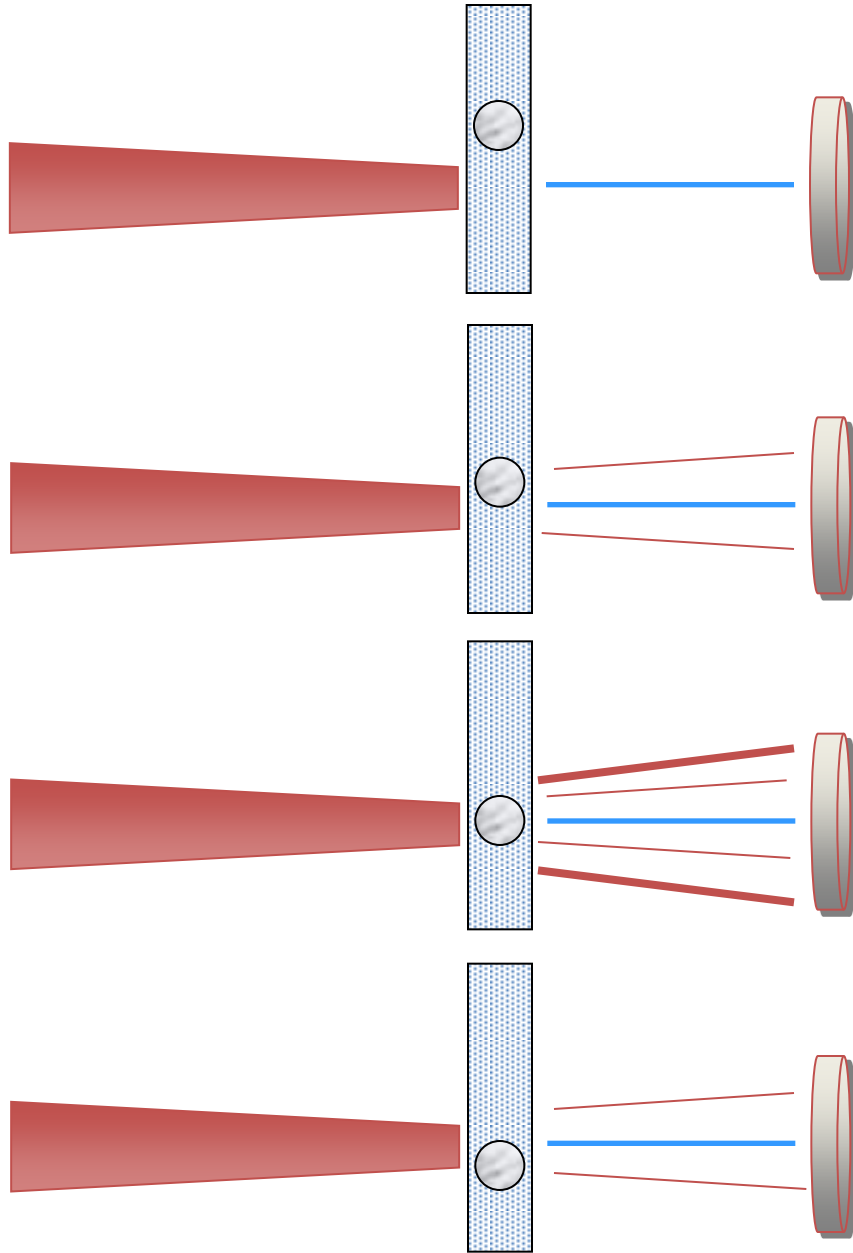
- Linear amplification is used when there is not such a broad range of signals e.g. in DNA analysis and calcium flux measurement.

# Log Amplifiers

- The use of a log amp is beneficial when there is a broad range of fluorescence as this can then be compressed; this is generally true of most biological distributions.



# The Voltage Pulse

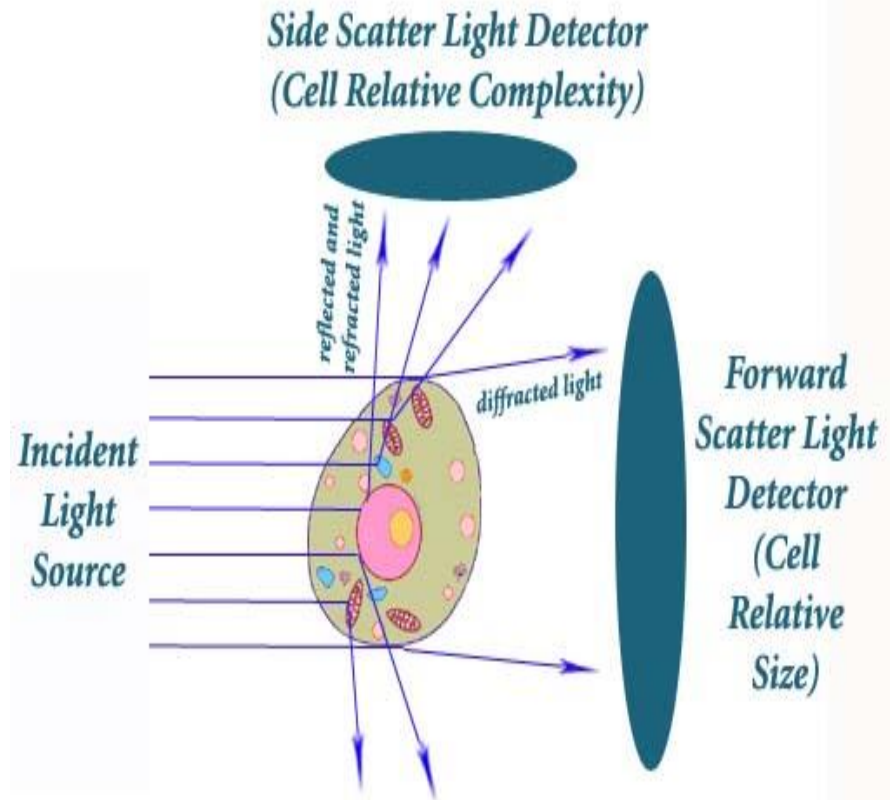


# Electronics Recap

- The varying number of photons reaching the detector are converted to a proportional number of electrons
- The number of electrons exiting a PMT can be multiplied by making more electrons available to the detector (increase Voltage input)
- The current generated goes to a log or linear amplifier where it is amplified (if desired) and is converted to a voltage pulse

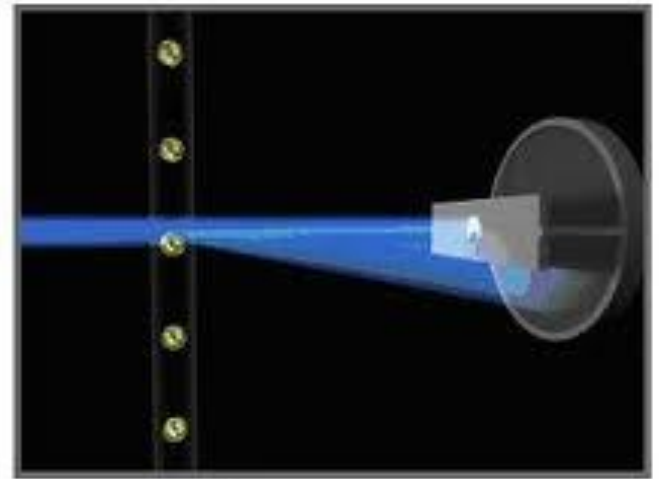
# Light Scatter

- When light from a laser interrogates a cell, that cell scatters light in all directions.
- The scattered light can travel from the interrogation point down a path to a detector.



# Forward Scatter

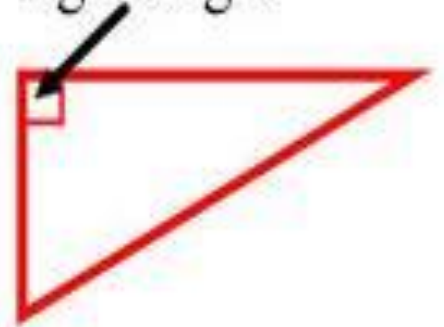
- Light that is scattered in the *forward* direction (along the same axis the laser is traveling) is detected in the Forward Scatter Channel.
- The intensity of this signal has been attributed to cell size, refractive index (membrane permeability)
- **Forward Scatter=FSC**



# Side Scatter

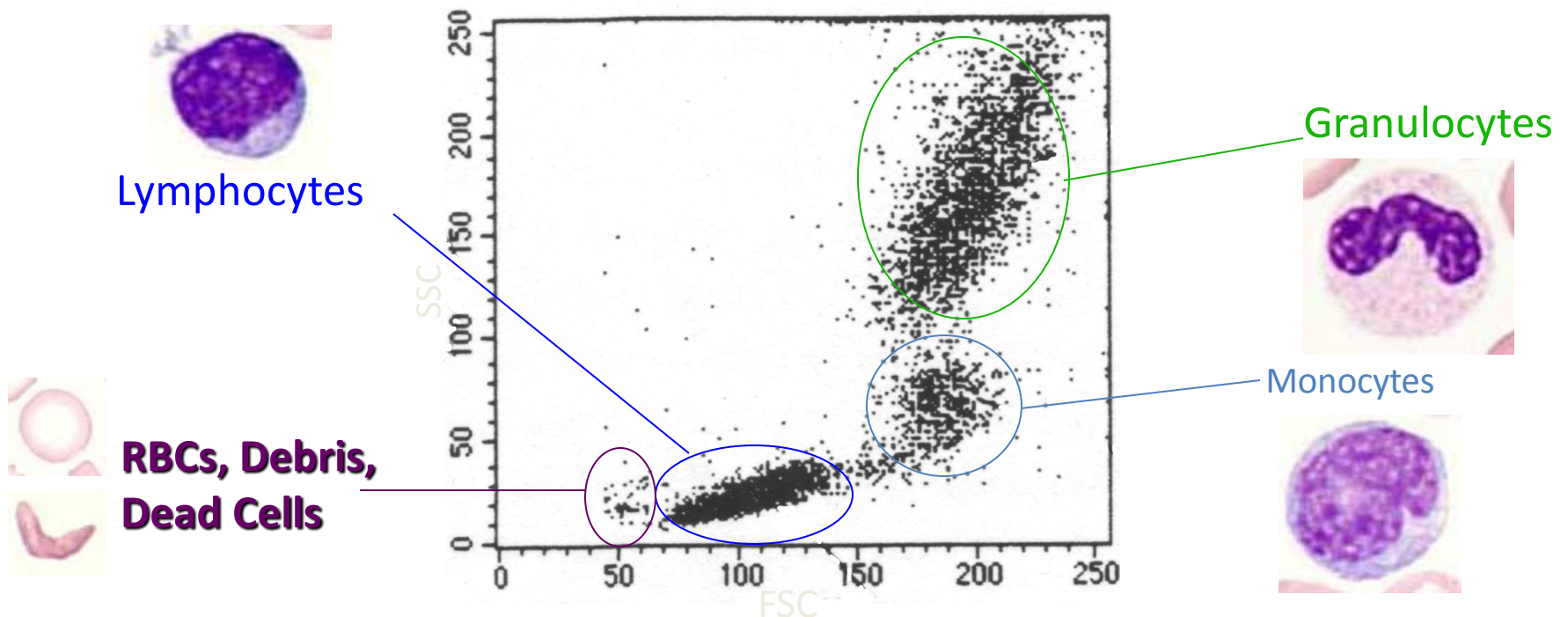
- **Laser light** that is scattered at 90 degrees to the axis of the laser path is detected in the Side Scatter Channel
- The intensity of this signal is proportional to the amount of cytosolic structure in the cell (eg. granules, cell inclusions, etc.)
- **Side Scatter=SSC**

right angle

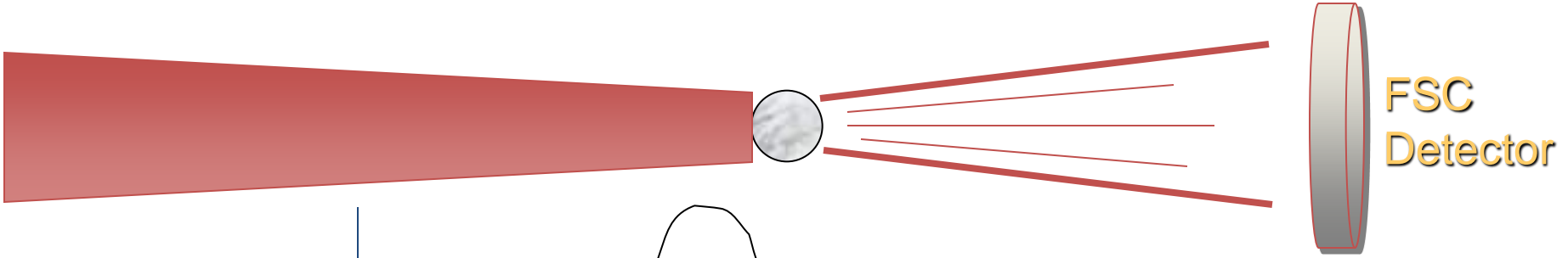


# Why Look at FSC v. SSC?

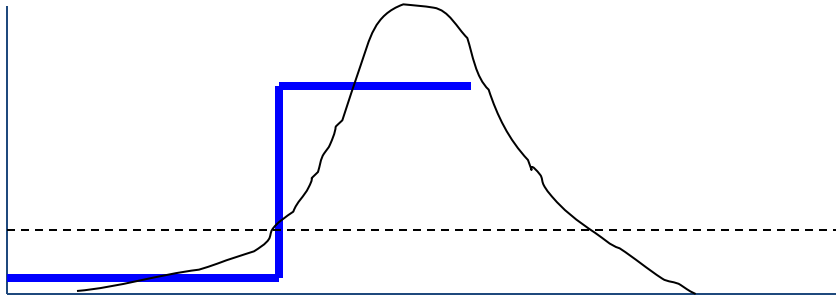
- Since FSC  $\sim$  size and SSC  $\sim$  internal structure, a correlated measurement between them can allow for differentiation of cell types in a heterogeneous cell population.



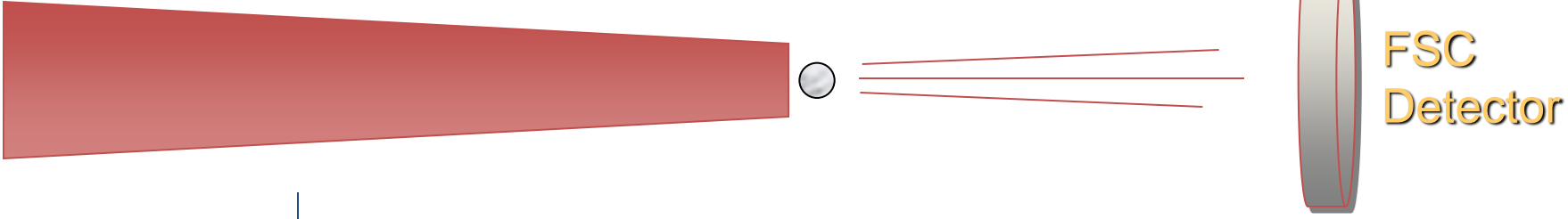
# Threshold



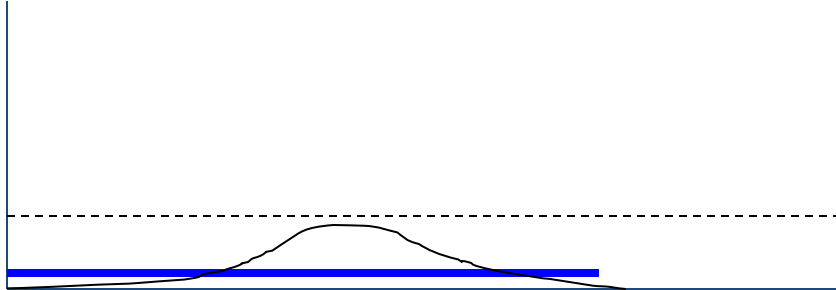
Threshold  
(eg. 52)



Time

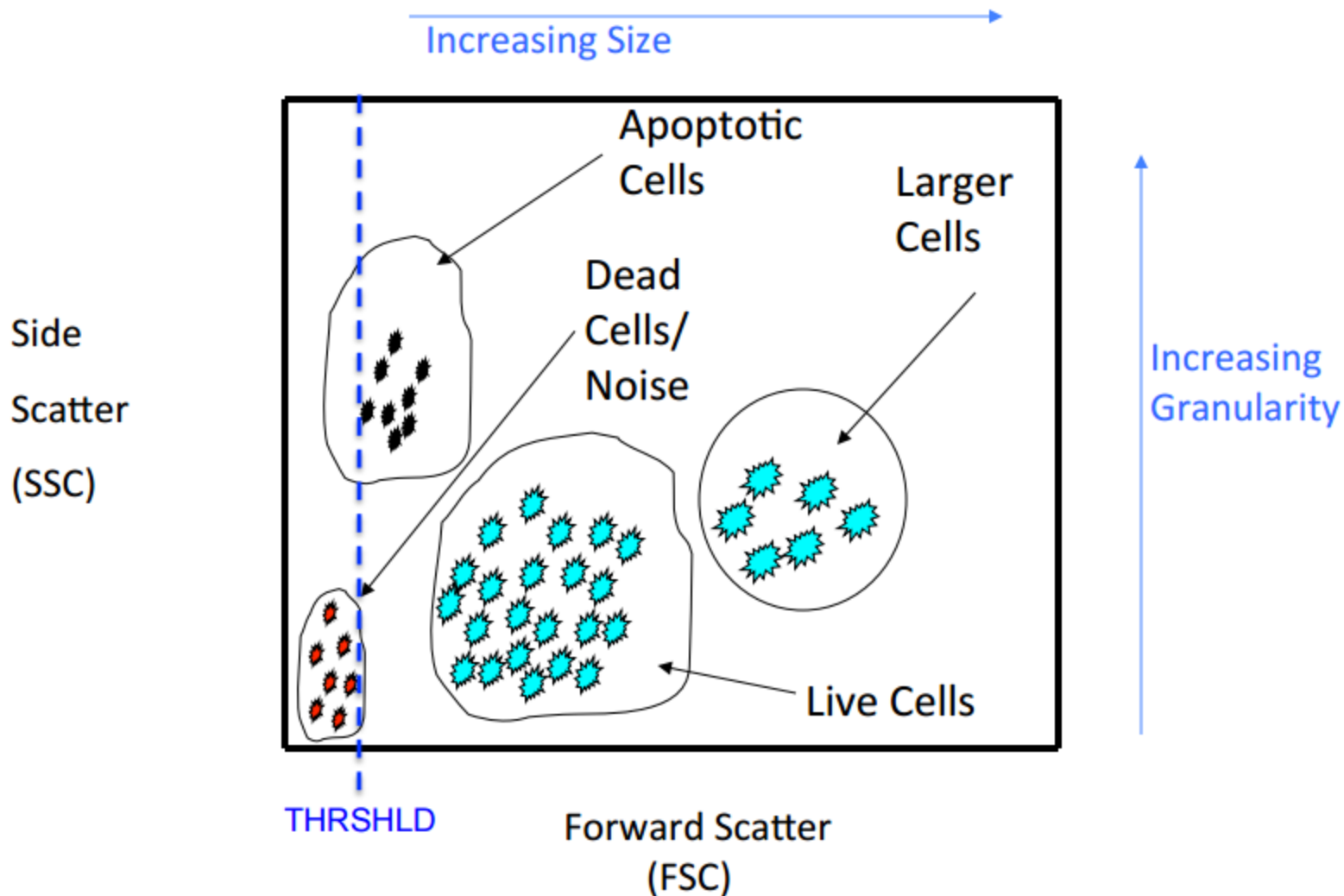


Threshold  
(eg. 52)



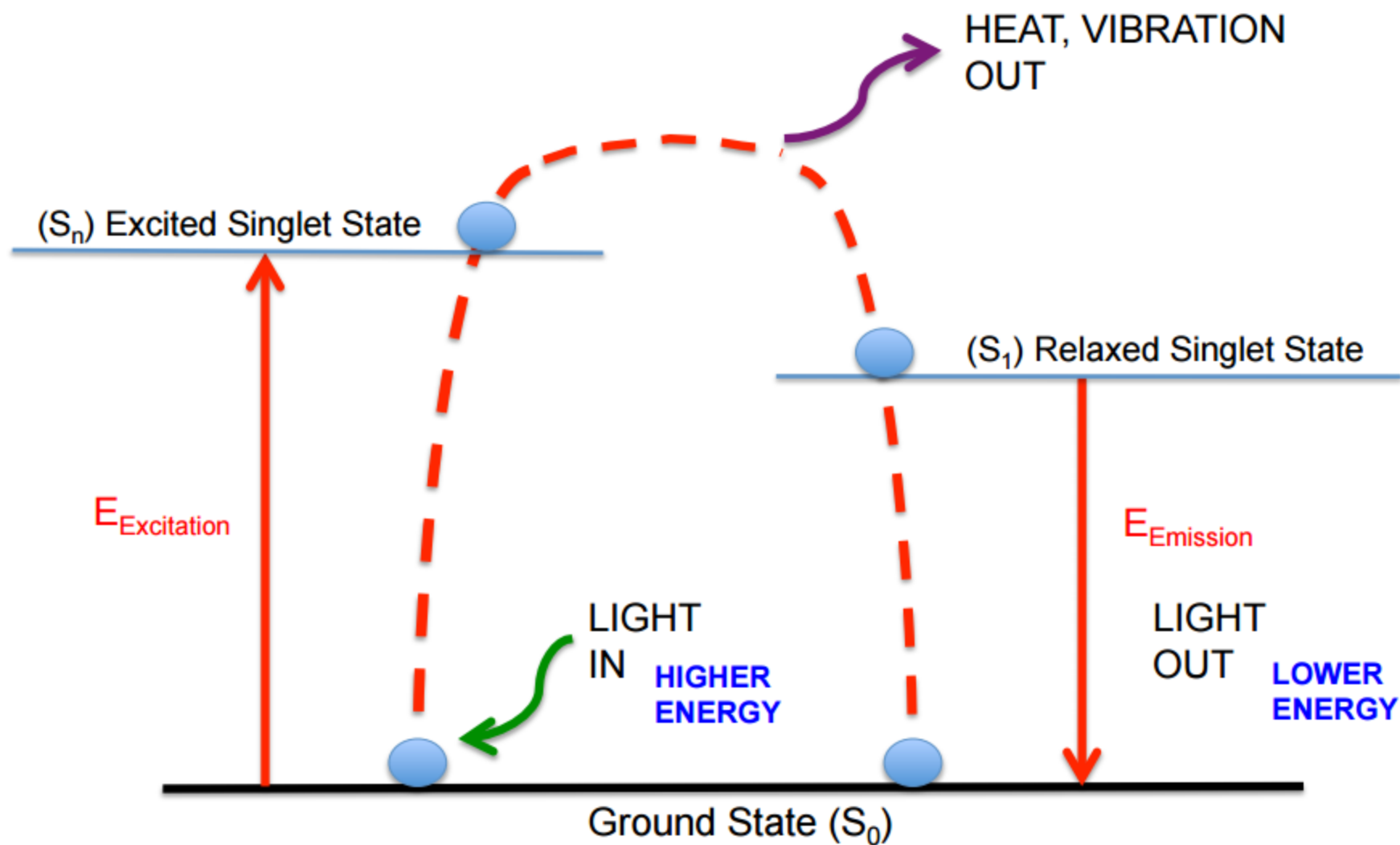
Time

# Typical Scatter Display





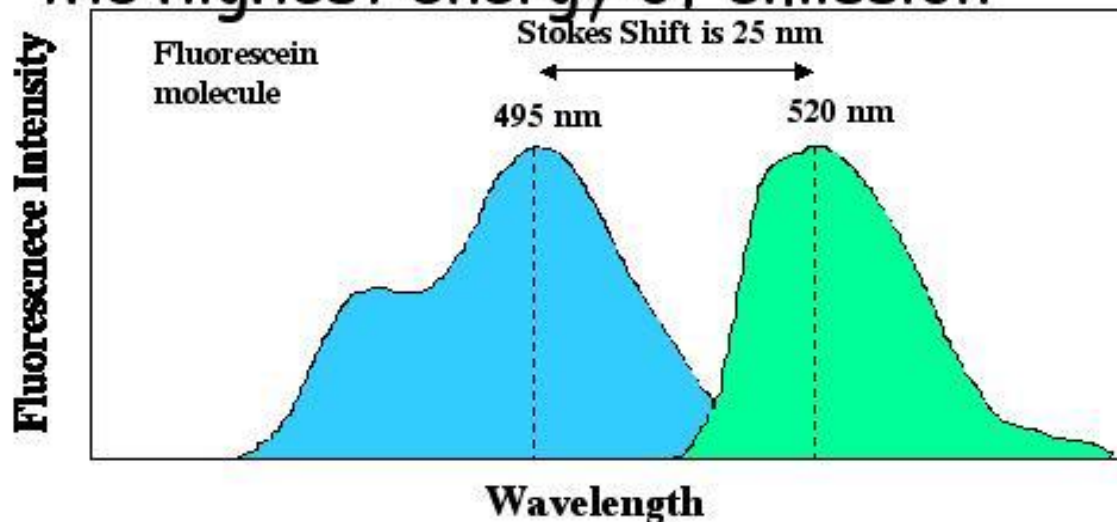
# Fluorescence: Electronic Energy Transition



# Fluorescence

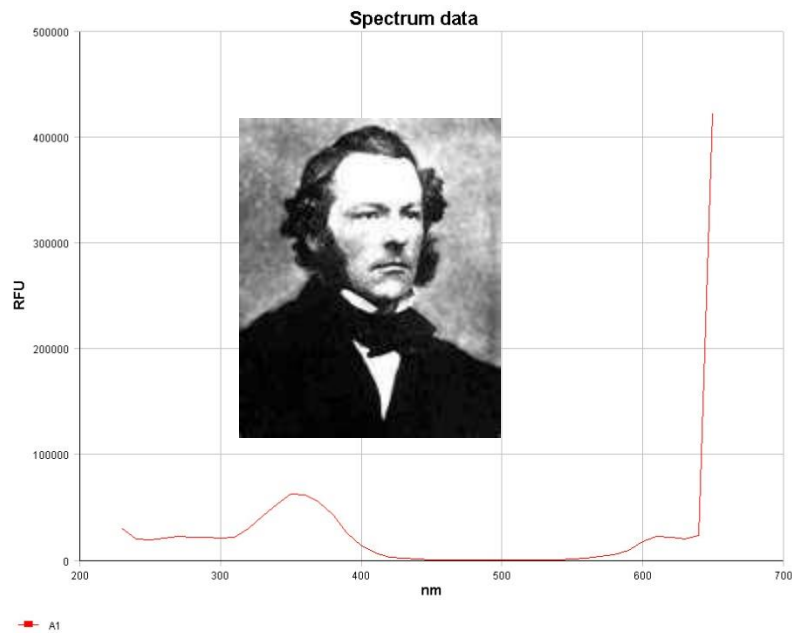
- **Stokes Shift**

- is the energy difference between the lowest energy peak of absorbance and the highest energy of emission

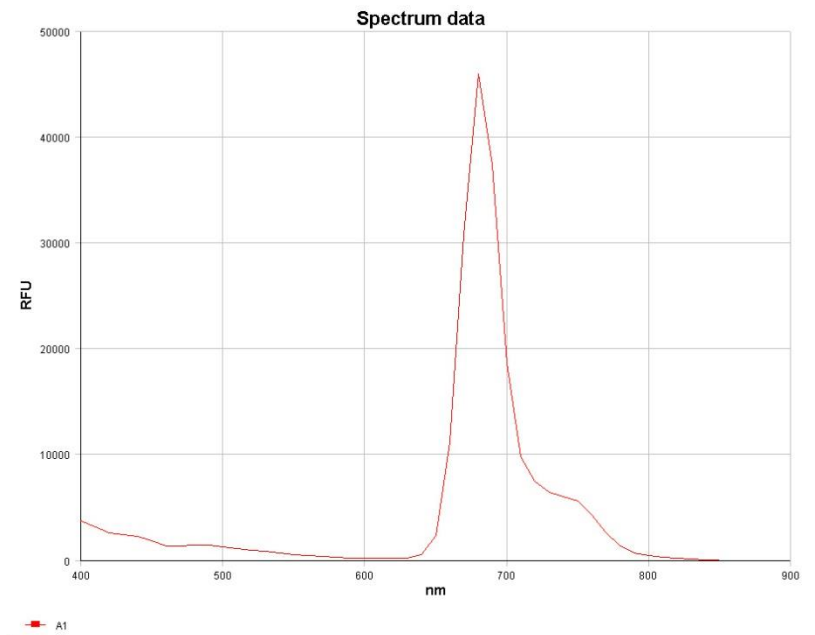


# Spectral Properties

## EXCITATION



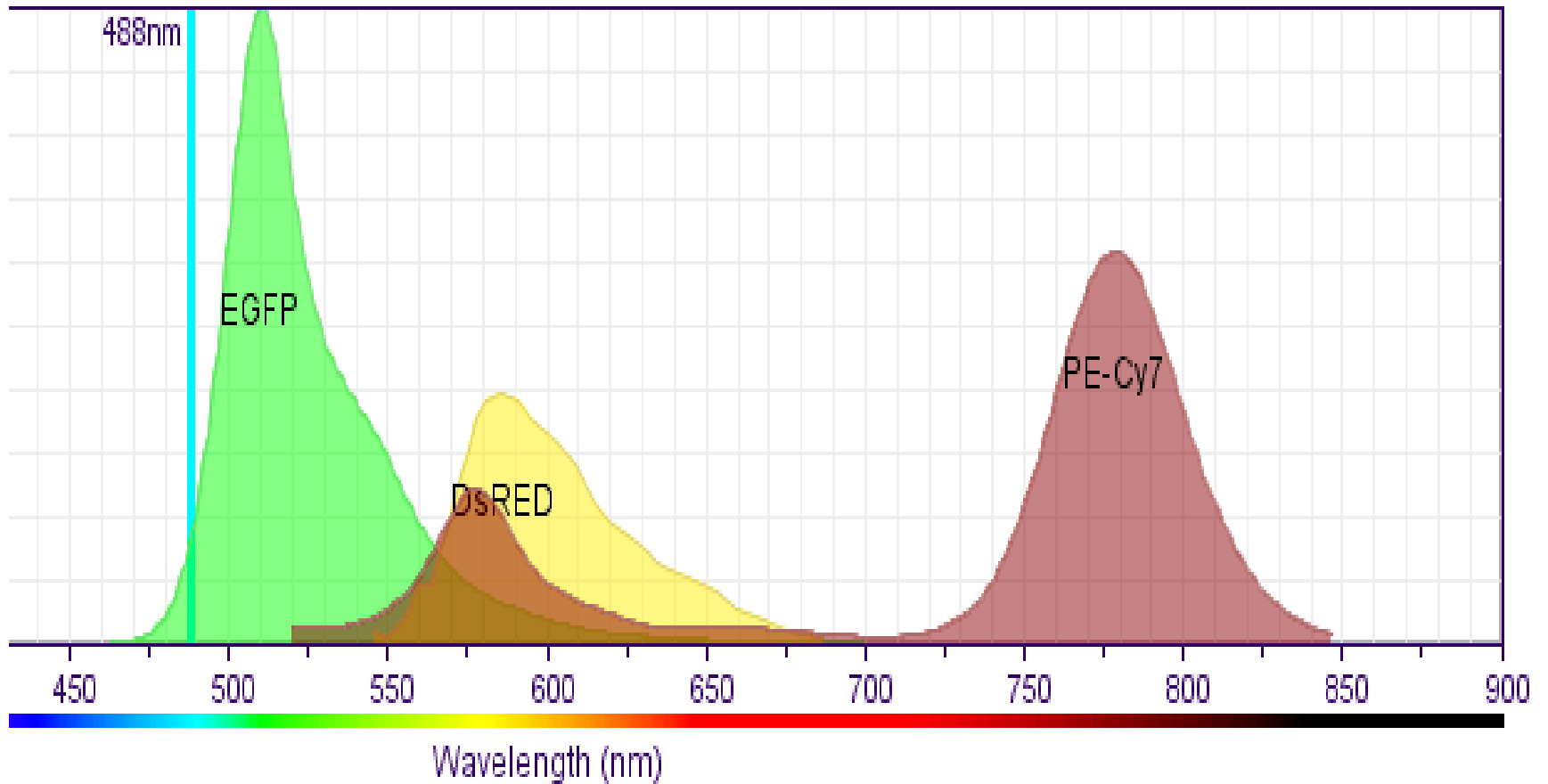
## EMISSION



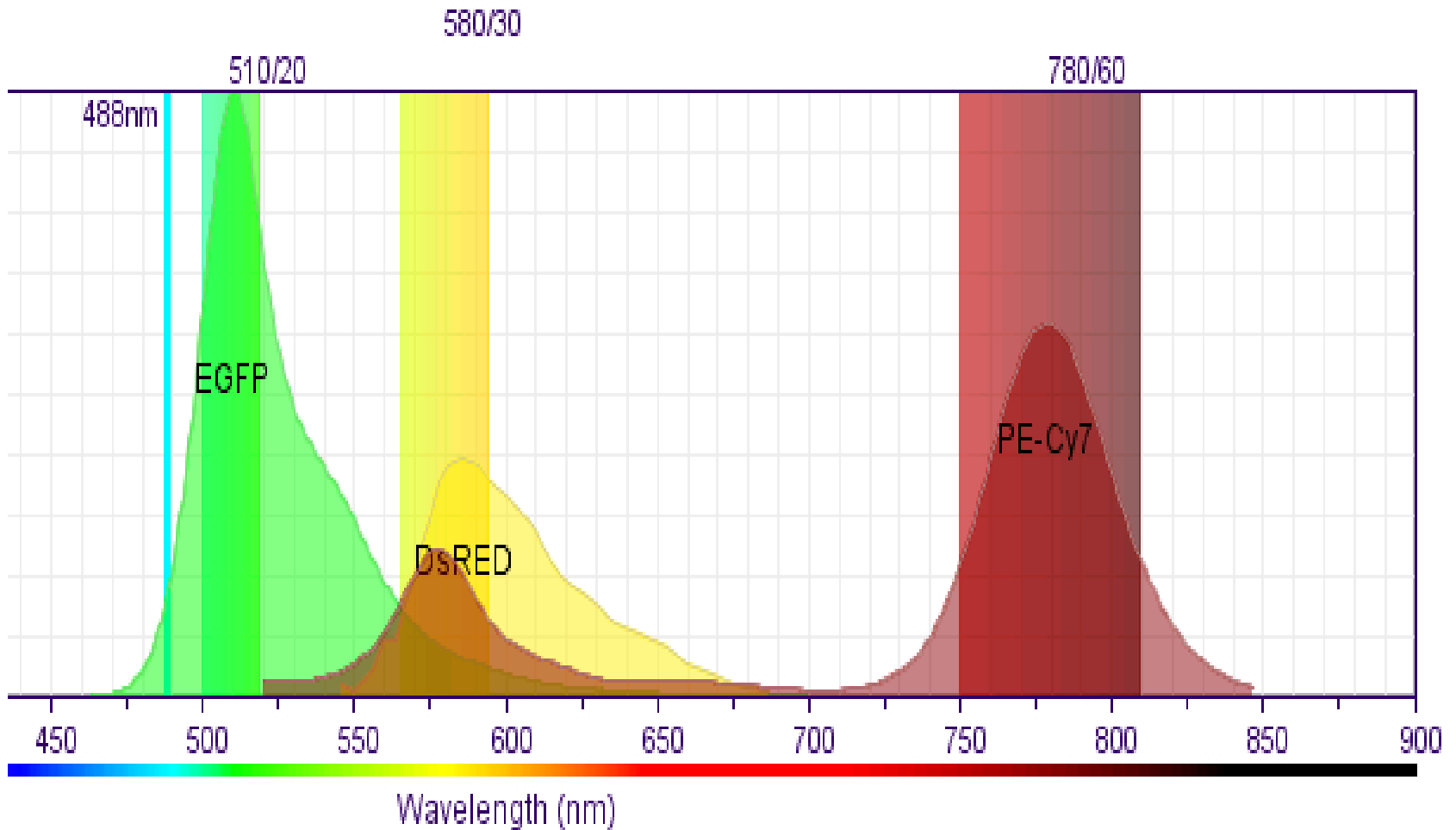
# Interrogation Recap

- A focused light source (laser) interrogates a cell and scatters light
- That scattered light travels down a channel to a detector
- FSC  $\sim$  size and cell membrane shape
- SSC  $\sim$  internal cytosolic structure
- Fluorochromes on/in the cell will become excited by the laser and emit photons
- These photons travel down channels and are steered and split by dichroic (LP/SP) filters
- Specific wavelengths are then detected by PMTs that have a filter in front of them

# SPECTRAL OVERLAP

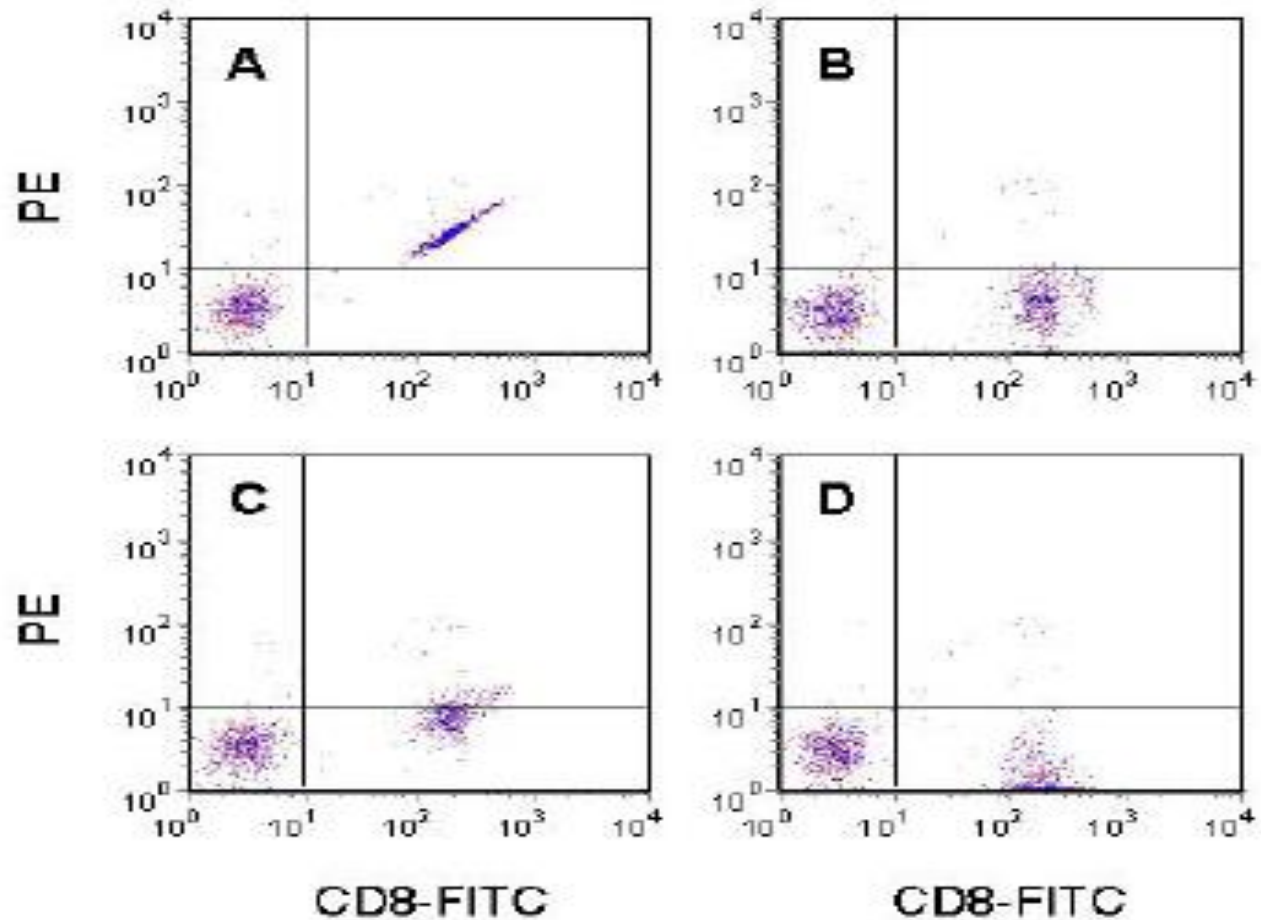


# BANDPASS FILTERS *HELP*



# COMPENSATION

Compensation is the process by which the fluorescence “spillover” originating from a fluorochrome other than the one specified for a particular PMT detector is subtracted as a percentage of the signal from other PMT’s.



Human peripheral blood lymphocytes labelled with CD8-FITC showing the CD4 -ve cells only. **A.** Uncompensated data. **B.** Correctly compensated. **C.** Under compensated. **D.** Over compensated.



# Mario Roederer's COMP Recipe

- (1) The compensation tube must consist of cells that are unstained as well as cells that are singly-stained with the fluorescent probes. The stained (positive) cells must have the same autofluorescence (when they are unstained) as do the unstained (negative) cells in the compensation tube (e.g., all are lymphocytes).
- (2) The PMT voltages must be set high enough guarantee that the negative population is off the axis in every channel.
- (3) An analysis gate is set so that only cells with identical autofluorescence characteristics are viewed (e.g., a lymphocyte gate). An analysis gate is also set to include all of the negative cells and all of the positive cells.
- (4) The centers of the positive and negative cell populations are aligned by matching the median fluorescences.